

RESEARCH ARTICLE

Open Access



Validity and reliability of serratus anterior hand held dynamometry

Jos IJspeert^{1*} , Hans C. J. W. Kerstens^{2,4}, Renske M. J. Janssen¹, Alexander C. H. Geurts¹, Nens van Alfen³ and Jan T. Groothuis¹

Abstract

Background: Strength testing of the serratus anterior muscle with hand held dynamometry (HDD) in supine subjects has low reproducibility, and is influenced by compensatory activity of other muscles like the pectoralis major and upper trapezius. Previously, two manual maximum voluntary isometric contraction tests of the serratus anterior muscle were reported that recruited optimal surface electromyography (sEMG) activity in a sitting position. We adapted three manual muscle tests to make them suitable for HDD and investigated their validity and reliability.

Methods: Twenty-one healthy adults were examined by two assessors in one supine and two seated positions. Each test was repeated twice. Construct validity was determined by evaluating force production (assessed with HDD) in relation to sEMG of the serratus anterior, upper trapezius and pectoralis major muscles, comparing the three test positions. Intra- and interrater reliability were determined by calculating intra-class correlation coefficients (ICC) smallest detectable change (SDC) and standard error of measurement (SEM).

Results: Serratus anterior muscle sEMG activity was most isolated in a seated position with the humerus in 90° antelexion in the scapular plane. This resulted in the lowest measured force levels in this position with a mean force of 296 N (SEM 15.8 N). Intrarater reliability yielded an ICC of 0.658 (95% CI 0.325; 0.846) and an interrater reliability of 0.277 (95% CI -0.089; 0.605). SDC was 127 Newton, SEM 45.8 Newton.

Conclusion: The results indicate that validity for strength testing of the serratus anterior muscle is optimal with subjects in a seated position and the shoulder flexed at 90° in the scapular plane. Intrarater reliability is moderate and interrater reliability of this procedure is poor. However the high SDC values make it difficult to use the measurement in repeated measurements.

Keywords: Muscle strength dynamometer, Strength testing, Reproducibility of results, Serratus anterior, Scapula

Background

The ability to stabilize the scapula against the chest wall at rest and during upper limb movement has been widely recognized as a prerequisite for optimal upper limb function and related daily activities [1, 2]. Scapular dyskinesis, defined as abnormal scapular position and movement that may result in e.g. ‘winging’ or ‘tipping’, has been observed in many types of shoulder pathology, such as impingement syndrome, rotator cuff and labral tears, glenohumeral instability, and secondary to central and peripheral nervous system disorders [3–6]. Several

authors have related scapular dyskinesis to loss of muscle strength in the scapulothoracic muscles, such as the lower and middle parts of the serratus anterior muscle [7–9]. Lack of strength or endurance in this muscle can cause downward (medial) rotation of the scapula, making its lower medial border more prominent [10]. Others have related scapular dyskinesis to a muscular imbalance (or discoordination) rather than muscle weakness [2, 6, 11]. Yet, various rehabilitation programs promote scapular strengthening exercises in the treatment of patients with shoulder disorders [12, 13]. However, reference values for serratus anterior muscle strength are not available. In addition, a strength training approach may not be beneficial for patients who have coordinative problems [14–16]. In this perspective,

* Correspondence: jos.ijspeert@radboudumc.nl

¹Department of Rehabilitation, Donders Institute for Brain, Cognition and Behaviour, Radboud University Medical Center, Nijmegen, the Netherlands
Full list of author information is available at the end of the article



it is important to test serratus anterior muscle strength and coordination separately in order to differentiate between patients who can and those who cannot benefit from strength training. The presence of scapular dyskinesis in the absence of strength loss would suggest that motor control therapy might be a more successful approach than strength training.

Manual muscle strength is routinely scored using a six point scale described by the Medical Research Council (MRC) [17]. Although the use of the MRC scale is widespread, its usefulness and reliability is questionable, particularly around joints other than the elbow and knee [18, 19]. Especially the evaluation of relatively normal muscle strength within the upper ranges of the MRC scale lacks interrater reproducibility [18], which is understandable as the definitions of the MRC grades imply that grade 3 is a fixed point ('anti-gravity strength'), but grade 4 is a wide range between grade 3 and 'normal' muscle strength (grade 5) [17]. Handheld dynamometry (HHD) was demonstrated to be a reliable alternative for MRC testing of muscle strength [20–22]. Reliability of HHD has been found to be high for the serratus anterior and trapezius muscles, although its validity with regard to these muscles has not been extensively studied [23].

Serratus anterior muscle strength is commonly evaluated by applying axial pressure to the humerus in the frontal plane with subjects in a supine position and their scapula protracted with 90° of anteflexion in the shoulder [24]. Due to the protraction, the supine test position might be prone to recruiting muscle activity in the pectoralis muscles and therefore not suited for measuring isolated serratus anterior muscle strength [24, 25]. Evaluation of serratus strength using active horizontal abduction during testing to correct for pectoralis activation is possible [26], however not feasible in clinical practice. Ekstrom et al. presented a different approach to the evaluation of maximum voluntary isometric contraction (MVIC) of the serratus anterior muscle. Their subjects were sitting upright with lumbar support, the arm positioned in the scapular plane and in 90° or 125° anteflexion of the shoulder [27]. In these two positions resistance was applied in the scapular plane at the olecranon and at the inferior angle of the scapula attempting to rotate the scapula downward (medially) [27]. They reported significantly higher surface electromyography (sEMG) activity of the serratus anterior muscle during MVIC testing in both seated positions compared to the supine position [27]. However, the two seated testing positions presented might also lack validity. The force needed for the serratus test above 90° in the scapular plane can produce co-contraction of the trapezius descendens muscle [25, 28]. Therefore, the strength

found in these positions is most likely not produced by the serratus anterior muscle alone.

To allow valid and reliable strength testing of the serratus anterior muscle with HHD, we modified both seated test positions described by Ekstrom et al. [27]. This modification was needed because the original tests required two points of contact, whereas HHD is only possible with one point of contact. Because of the lack of reference values it was not possible to compute a reasonable force production expected for these test positions. Therefore, construct validity was determined in healthy adult subjects, during MVIC testing, by evaluating sEMG activity of the serratus anterior, upper trapezius and pectoralis major muscles for the two modified seated positions compared to the supine position. We hypothesize that the position with the most isolated serratus anterior muscle EMG activity constitutes the most valid test for serratus anterior strength. In addition, for force measurements with HHD, intra- and interrater reliability of each test position were evaluated by comparing repeated measurements by two assessors.

Methods

This study was approved by the medical ethical committee of the Radboud University Medical Center and complied with the declaration of Helsinki. Written informed consent was obtained from each subject before inclusion in this study.

Subjects

Twenty-one healthy subjects were recruited by convenience sampling from physical therapy students of the University of Applied Sciences in Nijmegen, the Netherlands.

Inclusion criteria were: age 18 years or older and sufficient knowledge of the Dutch or English language to understand written and spoken instructions. Exclusion criteria were: rotator cuff tendinopathy or tears, other glenohumeral or subacromial deficits, rheumatic diseases, central or peripheral nervous system disorders, acute shoulder pain before or during the experiment. All above criteria related to the tested arm (right side), if applicable.

Experimental protocol

We examined three different positions (A, B and C) to test the muscle strength of the serratus anterior. Test position A is a frequently used evaluation of serratus anterior muscle strength described by Michener et al. [24]. In supine position, subjects are required to resist strength applied by the HHD placed just below the olecranon, while placing the elbow and the shoulder in 90° flexion in the frontal plane. Test positions B and C have been derived from Ekstrom et al. and adapted for use with HHD [27]. Subjects are seated in a stable chair with lumbar support, but without scapular support. They are instructed to

elevate the tested arm in the scapular plane to respectively 90° and 125° shoulder flexion, with the elbow in 90° of flexion. Angles were checked with a standard goniometer. Axial pressure was applied with the HDD on the olecranon in the scapular plane. In test positions B and C, assessors placed themselves against a wall for extra stability and strength, in contrast to position A. (see Fig. 1).

Measurements

Subjects were tested during one day in the morning and afternoon. All subjects refrained from any sports activity on the day of testing.

For strength and sEMG measurements the ‘make method’ for strength testing was used [29]. MVIC testing was carried out by two assessors, both experienced physical therapists (JL, 30 yrs., 115 kg, 192 cm; and HK, 40 yrs., 76 kg, 183 cm). Calibrated Microfet II™ HHDs were used for the collection of strength data. A test assistant stored the sEMG output as well as the strength data in Newton on a computer. The assessors were not able to read out strength data or sEMG signals during testing. Per test position, each contraction lasted 3 s with a ramp up of 4 s and a ramp down of 4 s. Starting cues for timing of the tests were given by the test assistant. The assessors instructed subjects as follows: after the given cue for start of measurement, they counted down from 4 to 0, after which the subject was asked to “push-push-push” for 3 s and then asked to gradually release strength while counting down from 4 to zero. Each contraction was repeated twice per test position, with at least one-minute rest between trials. Every subject was tested twice by each assessor, with a two-minute resting period in between, in test positions A, B and C.

EMG setup

Surface EMG signals were collected from the serratus anterior, upper trapezius and pectoralis major muscles by applying wireless sensors (W4p-SP-W01, Delsys Inc., Boston, USA) to the skin with Delsys Adhesive Sensor Interface. Prior to electrode placement, the skin was carefully shaved, degreased with alcohol and rubbed with sanding paper. The sEMG sensors were placed at the following locations: for serratus anterior muscle measurement at the 6th to 8th rib in the mid-axillary line anterior to the fibers of the latissimus dorsi muscle [27]; for upper trapezius muscle measurement at 50% on the line from the acromion to the C7 spinous process, following SENIAM guidelines [30]; and for the pectoralis major muscle measurement electrodes were placed approximately 2 cm medial to the coracoid process (Fig. 1, [28, 30]).

Data analysis

The sEMG signals were filtered and rectified (low cut-off filter 10 Hz, high-cut off filter 1000 Hz, notch filter at 50 Hz), digitized at a sampling rate of 2000 Hz with a common mode rejection ratio of > 80 dB (W4p-SP-W02, Delsys Inc., Boston, USA), and were stored on a laboratory computer for offline analysis. During offline analysis, the root mean square (RMS) of the sEMG signals during the three second maximum for each contraction were calculated using EMG Works® (Delsys Inc., Boston, USA). Subsequently, the signals of the 2 contractions per test position were averaged per assessor. Strength data was recorded in Newtons.

Statistical analysis

Validity

Statistical analysis was performed using Statistical Analysis System 9.2 (SAS Institute Inc., Cary, USA). Inspection of



Fig. 1 Test positions and surface electromyography placements for serratus anterior muscle testing, note; depicted angles differ from actual goniometry angles measured while testing. **a** 90° of shoulder flexion in the frontal plane. **b** 90° of shoulder flexion in scaption. **c** 125° of shoulder flexion in scaption

sEMG data revealed a non-normal distribution. Therefore, a logarithmic transformation was performed to correct for skewness. A linear mixed model for repeated measurements was used to assess the differences between the three test positions for each muscle, separately. The model reference point was set at test position C, as it was estimated that this test position would produce most serratus anterior muscle activity based on the study by Ekstrom et al. [27]. The dependent variable was the logarithmically transformed RMS-value of EMG activity during the 3-s maximum contraction. The estimated values of the sEMG activity for each position and the relative differences between the positions with 95% confidence intervals (CIs) were calculated by use of the anti-logarithmic transformation.

Reliability

Strength data was also inspected for normality. The difference in muscle force (N) between the test and the re-test measured by JI, and between tester JI and HK was calculated. Reproducibility (test-retest) was divided into assessment of reliability and agreement parameters [31]. Reliability was analysed using the intraclass correlation coefficient (ICC). ICC's were calculated using a two-way mixed effect model (ICC3.1agreement) with 95% confidence intervals (CI). ICC values were interpreted as follows in terms of reliability: < 0.5 as "poor", 0.5–0.75 as "moderate", 0.75–0.9 as "good", and > 0.9 as "excellent" [32]. To assess agreement, the standard error of measurement (SEM agreement) and the smallest detectable change (SDC agreement) were calculated. Both were expressed in the unit of the measurement, Newton. The

Table 1 linear mixed models of electromyography activity difference estimations

Model	Effect	Estimate	95% CI	
			LL	UL
Serratus anterior	Intercept (mV)	239.54	173.78	330.13
	Pos A	1.09	.78	1.38
	Pos B	1.02	.81	1.24
	Pos C	1	–	–
Pectoralis minor	Intercept (mV)	33.04	23.23	45.04
	Pos A	2.94	2.13	4.05
	Pos B	1.32	.96	1.83
	Pos C	1	–	–
Trapezius descendens	Intercept (mV)	89.88	28.34	53.82
	Pos A	.43	.29	.65
	Pos B	.63	.42	.95
	Pos C	1	–	–

Legend: 95% CI, 95% confidence interval; LL, Lower limit; UL, upper limit; mV, microvolts; Pos A, test position A; Pos B, test position B; Pos C, test position C (reference)

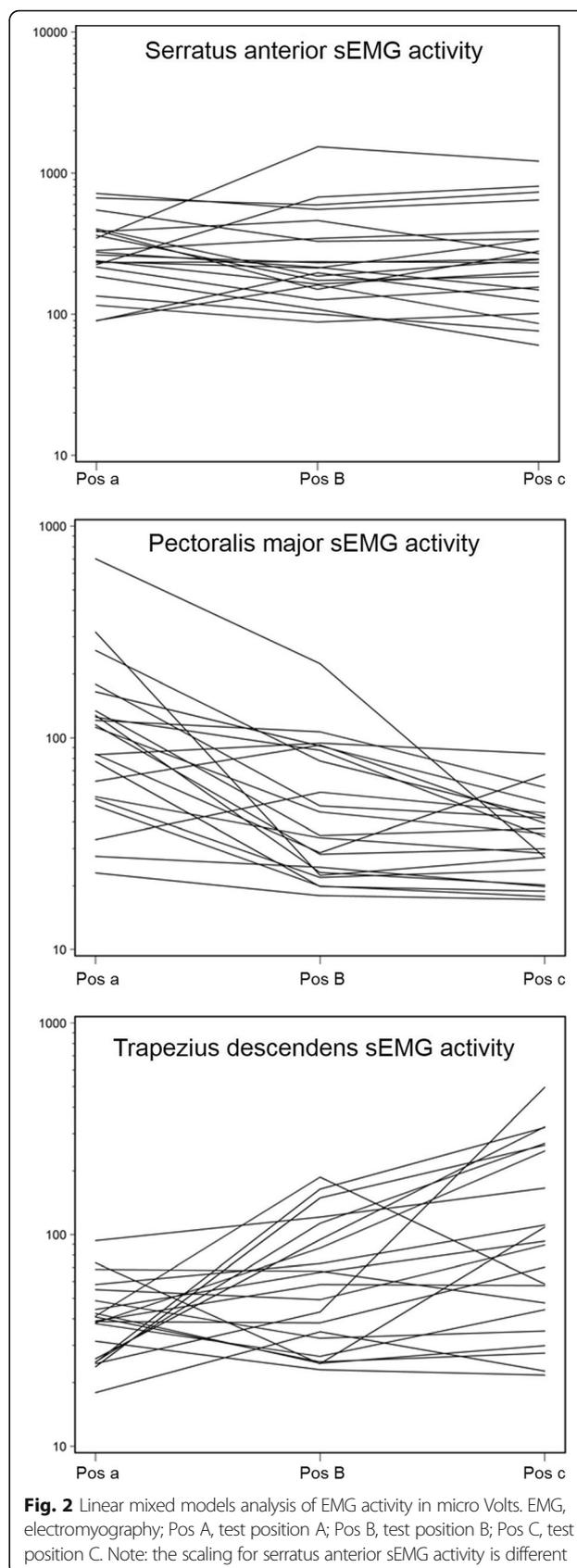


Fig. 2 Linear mixed models analysis of EMG activity in micro Volts. EMG, electromyography; Pos A, test position A; Pos B, test position B; Pos C, test position C. Note: the scaling for serratus anterior sEMG activity is different

SEM was calculated as $SEM_{agreement} = p\sigma^2_{error} = p(\sigma^2_o + \sigma^2_{residual})$ [33]. The variance due to systematic differences between the observers (σ^2_o) and the residual variance ($\sigma^2_{residual}$) were obtained through a varcomp analysis [33]. The SEM agreement was used to calculate the SDC agreement = $1.96 \times p \times SEM$ [30]. In this formula 'n' refers to the number of measurements, which is two in our study for test-retest reliability and inter-tester reliability [30]. Bland-Altman plots were constructed to determine if there was bias in measurement error [34, 35]. This plot shows the rater difference against the mean muscle force. The plot visualizes the relationship between the measurement error and the observed value including the presence of systematic bias and bias related to the magnitude of serratus anterior strength. The 95% limits of agreement (95% LoA) were shown in the plot (mean difference ± 1.96 SD). All analyses were performed using IBM SPSS Statistics v22 (SPSS Inc., Chicago, Illinois, United States).

Results

We included 21 subjects (15 males; 19 right-handed) with a mean age of 21 years (range 19–32) and a mean (\pm SD) BMI of 22.7 ± 2.1 kg/m². Mean forces (\pm SEM) measured per test position were: position A 369.8 ± 18.3 N; position B 296.0 ± 15.8 N; and position C 313.0 ± 19.8 N.

sEMG activity of the serratus anterior muscle was very similar between the three different test positions. However, the pectoralis major muscle showed significantly more activity in position A compared to B and C, and the upper trapezius muscle showed significantly more activity in position C compared to A and B (see Table 1, Fig. 2).

ICC values and agreement parameters for test-retest and interrater reliability of test positions A, B and C are reported in Table 2.

Paired samples t-tests for the difference scores between HK en JI, were significantly different ($p > 0.05$), showing no agreement between these different raters. Therefore Bland-Altman plots were only presented for the test-retest data (Fig. 3).

Discussion

By using sEMG of the serratus anterior, upper trapezius and pectoralis major muscles we were able to demonstrate that the serratus anterior muscle was equally activated in three test positions, but most selectively in the seated position with the arm placed in 90° of flexion in the scapular plane (position B, Fig. 1). Position B produced less maximum strength compared to position A (- 74 N) and C (- 17 N), suggesting less co-contraction by the upper trapezius or pectoralis major muscles. Therefore, test position B seems to be the most valid position for isolated assessment of serratus anterior muscle strength measured with HDD. We found similar sEMG activity in all test positions, although we expected to measure most serratus anterior muscle activity in position C based on the previous study by Ekstrom et al. [27]. An important difference with the present study is that the original test provides the opportunity to apply resistance to the arm as well as the scapula using two hands. We used only one point of contact at the arm without scapular fixation, which can explain more similar serratus anterior muscle activity among test positions in our study. The idea of testing in the scapular plane is supported by a recent cadaver study, which has shown that the serratus anterior muscle fascicles from the 4th to 9th rib are attached to the inferior angle of the scapula [36]. The inferior angle of the scapula shows more movement when the arm moves in the scapular plane than in the frontal plane [37]. This confirms that serratus anterior muscle strength should be tested in the scapular plane.

Table 2: test-retest and interrater reproducibility of serratus anterior hand held dynamometer strenght testing

	Test (N) mean (SD)	Retest (N) mean (SD)	Diff test-retest (N) mean (SD)	95% LoA (N)	ICC3.1 _{agreement} (95 % CI)	SEM _{agreement} (N)	SDC _{agreement} (N)
<i>test-retest</i>							
Pos A	383.88 (77.65)	404.92 (84.96)	-21.05 (60.22)	-139.08; 96.98	0.712 (0.420; 0.871)	44,10	122,40
Pos B	314.43 (75.1)	322.34 (82.34)	-7.90 (65.90)	-137.06; 121.26	0.658 (0.324; 0.846)	45,80	127,00
Pos C	351.54 (100.36)	376.16 (93.55)	-24.62 (59.37)	-140.99; 91.75	0.794 (0.490; 0.916)	44,52	123,40
	<i>Tester JI</i>	<i>Tester HK</i>	<i>Diff Tester JI VS HK</i>				
<i>Interrater</i>							
Pos A	383.88 (77.65)	340.44 (82.95)	43.43* (92.74)	-138.34; 225.20	0.794; (0.552; 0.912)	55,80	196,80
Pos B	314.43 (75.10)	264.21 (61.76)	50.21* (78.85)	-104.34; 204.76	0.277 (-0.089; 0.605)	55,80	154,50
Pos C	351.54 (100.36)	265.10 (40,0)	86.48* (86.21)	-82.49; 255.45	0.226 (-0.107; 559)	85,31	236,47

N Newton, SD Standard deviation, Diff Difference, LoA limits of agreement, ICC Intraclass correlation coefficient, CI Confidence interval, SEM Standard error of measurement, SDC Smallest detectable change, % percentage; *: $p < 0.001$

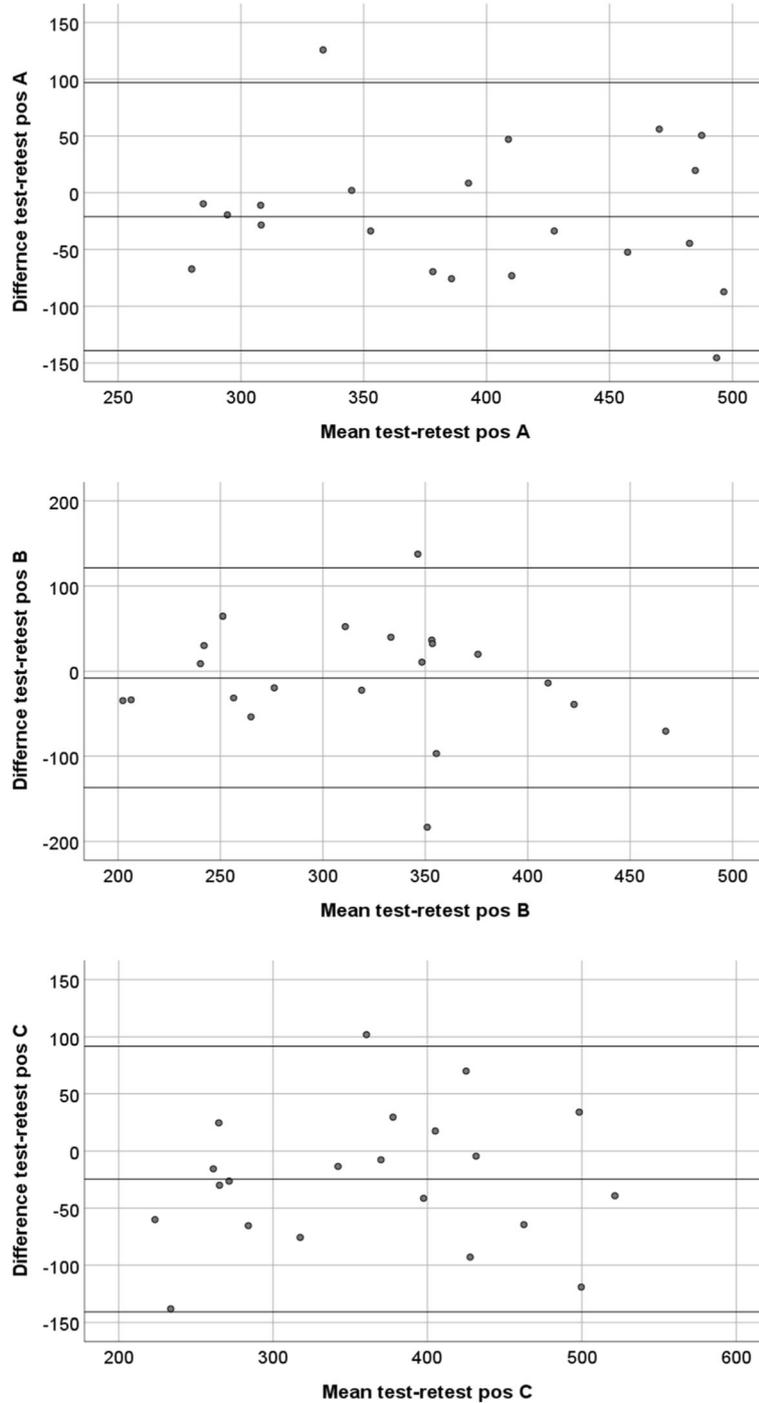


Fig. 3 Bland Altman plots for test-retest differences and their relation to the magnitude of strength measured with HHD in Newtons

We observed a moderate intrarater reliability (ICC3.1 agreement). Intrarater reliability of test position B was moderate, although somewhat lower than of position A, with an ICC of .658. Interrater reliability was poor with an ICC of .277. However, the SDC agreement and SEM agreement are rather large. The apparent contradiction between a moderate ICC 3.1 agreement

and high SDC agreement and SEM agreement is likely to be caused by the high heterogeneity in the population variance, which makes the random error and systematic error relatively lower. However, and SDC agreement of 127 N for the most valid test position (position B) makes it less fit for use in test-retest settings.

The interrater reliability shows low ICC 3.1 agreement. Moreover, the T-test difference in measurements done by HK and JI was significant ($P > 0.05$), so there is no agreement in these measurements (supported by even higher SDC agreement and SEM agreement scores).

The Bland-Altman plots did not show any systematic error in measurement, but did show increased difference scores in the high strength measurements.

We found relatively low intra- and interrater agreement in all our tests. Our subjects produced strength values exceeding 290 N. Although we tried to compensate for this by placing the assessor's arm holding the HHD against a wall in positions B and C, our approach may still have led to variation between raters resulting in only fair to moderate ICC values. Another factor may have been the different physical characteristics of the two assessors in our study, who had a substantial difference in body size and weight and therefore, possibly, a different ability to provide resistance to the subject's force production. When compared to the data reported by Michener et al., the ICC values found in the present study are relatively low [24], but the strength values are much higher (exceeding 290 N compared to around 150 N [24]). This may be caused by the fact that Michener et al. included subjects with shoulder pain, whereas we tested healthy young volunteers. It has previously been reported that the reliability of HHD decreases with strength testing levels above 120 N [38]. This may be due to the fact that assessors do not have sufficient strength to resist the force produced by the subject.

Translating our results to patients with shoulder problems, the reliability of the measurements is likely to improve in impaired subjects, because smaller amounts of strength are required from the assessor to counteract the serratus anterior muscle forces. Using a stabilization device, as was done in a study by Kolber et al., might also improve reliability, but will decrease the feasibility of the proposed testing protocol in clinical practice [39].

Our study had some limitations. First, we used sEMG instead of finewire-needle EMG signals, to avoid subject discomfort and for medical-ethical reasons. Although sEMG captures a larger number of motor units compared to finewire needle EMG, the use of surface electrodes might have resulted in cross-talk [40]. For instance, for the upper trapezius muscle, cross-talk might occur from the underlying supraspinatus muscle, and for the serratus anterior muscle from the intercostal muscles. Yet, studies by Fuglevand et al. and Winters et al. indicated that 90% of the sEMG signal is recorded from within 10–12 mm of the surface electrodes when an electrode spacing of 20 to 25 mm is used [40, 41]. In our setup this approach should have provided sufficient confidence to measure relatively isolated sEMG data from the serratus anterior, pectoralis major and trapezius descendens muscles, because the musculature possibly

causing cross-talk was located well away from this distance. Another limitation may have been the difference in physical characteristics between the two assessors in this study. However, such variations will also occur in regular clinical practice. Finally, the study group of 21 subjects falls short of the proposed 30 subjects or more by cosmin standards [42]. We feel that the validity part of the study has not suffered from the lower number of subjects.

Conclusion

We recommend to assess serratus anterior muscle strength manually, applying axial pressure to the humerus, with subjects in a seated position and with the shoulder flexed at 90° in the scapular plane. Given the relatively low agreement parameters, evaluation of treatment with HHD should preferably be done by the same assessor. Although further research validating this test procedure in patients with shoulder complaints and pathologies is needed, we expect it to be more feasible in populations with shoulder problems because of limited strength values in those groups.

Abbreviations

CI: Confidence interval; HHD: Hand held dynamometry; ICC: Intraclass correlation coefficient; MVIC: maximum voluntary isometric contraction; RMS: Root mean square; SEM: Standard error of the mean; sEMG: Surface electromyography

Acknowledgements

We would like to thank all participants. HAN university of applied sciences kindly provided measurement equipment and logistic support.

Suppliers

- Microfet II™ hand held dynamometers: HOGGAN Scientific, LLC
- Wireless electromyogram sensors: Delsys Inc., Boston, USA)

Authors' contributions

Jl was the primary researcher of this study, conceptualized the study, carried out measurements and wrote the manuscript under supervision of JG and NvA, HK assisted in recruitment of subjects, carried out measurements, analyzed EMG signals and contributed in writing the manuscript. RJ contributed in writing the manuscript and clinical interpretation. AG helped interpret the clinical relevance of the data and was a major contributor in writing of the manuscript. NvA conceptualized the study, helped interpret EMG data and was a major contributor in writing of the manuscript. JG conceptualized the study, helped interpret clinical relevance of the data and was a major contributor in writing of the manuscript. All authors read and approved the final manuscript.

Funding

This study was financially supported by the Dutch Rare Diseases Fund ('Zeldzame Ziekten Fonds'). The funding body had no role in conceptualizing the design of the study or collection, analysis, and interpretation of data or in writing the manuscript.

Availability of data and materials

The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request. The dataset has not been posted in an online depository.

Ethics approval and consent to participate

This study was approved of by our local medical ethics review board: 'CMO regio Arnhem Nijmegen'. Registration number: 2013/177. Written informed consent was collected from all participants.

Consent for publication

Written consent for publication for the pictures in figure one was obtained.

Competing interests

The authors declare that they have no competing interests.

Author details

¹Department of Rehabilitation, Donders Institute for Brain, Cognition and Behaviour, Radboud University Medical Center, Nijmegen, the Netherlands.

²Department of paramedical studies, HAN University of Applied Sciences, Nijmegen, The Netherlands.

³Department of Neurology and Clinical Neurophysiology, Donders Institute for Brain, Cognition and Behaviour, Radboud University Medical Center, Nijmegen, The Netherlands.

⁴IQ Healthcare, Radboud Institute for Health Sciences, Radboud University Medical Center, Nijmegen, The Netherlands.

Received: 15 March 2019 Accepted: 25 July 2019

Published online: 07 August 2019

References

1. Hebert LJ, Moffet H, McFadyen BJ, Dionne CE. Scapular behavior in shoulder impingement syndrome. *ArchPhysMedRehabil.* 2002;83(1):60–9.
2. Ludewig PM, Hassett DR, Laprade RF, Camargo PR, Braman JP. Comparison of scapular local coordinate systems. *Clin Biomech (Bristol, Avon).* 2010;25(5):415–21.
3. Paletta GA. Shoulder kinematics with two-plane x-ray evaluation in patients with anterior instability or rotator cuff tearing. *J Shoulder Elb Surg.* 1997;6(6):516–27.
4. Lukasiewicz AC, McClure P, Michener L, Pratt N, Sennett B. Comparison of 3-dimensional scapular position and orientation between subjects with and without shoulder impingement. *J Orthop Sports Phys Ther* 1999;29(10):574–583; discussion 84–6.
5. Warner JJP, Micheli LJ, Arslanian LE, Kennedy J, Kennedy R. Scapulothoracic motion in Normal shoulders and shoulders with Glenohumeral instability and impingement syndrome a study using Moire topographic analysis. *Clin Orthop Relat Res.* 1992;285:191.
6. Van Eijk JJ, Grootuis JT, Van Alfen N. Neuralgic amyotrophy: an update on diagnosis, pathophysiology, and treatment. *Muscle Nerve.* 2016;53(3):337–50.
7. Pink MM, Tibone JE. The painful shoulder in the swimming athlete. *Orthop Clin N Am.* 2000;31(2):247–61.
8. Glousman R. Electromyographic analysis and its role in the athletic shoulder. *Clin Orthop Relat Res.* 1993;(288):27–34.
9. Decker MJ, Hintermeister RA, Faber KJ, Hawkins RJ. Serratus anterior muscle activity during selected rehabilitation exercises. *Am J Sports Med.* 1999;27(6):784–91.
10. Watson CJ, Schenkman M. Physical therapy management of isolated serratus anterior muscle paralysis. *Phys Ther.* 1995;75(3):194–202.
11. Cools A, Declercq G, Cambier D, Mahieu N, Witvrouw E. Trapezius activity and intramuscular balance during isokinetic exercise in overhead athletes with impingement symptoms. *Scand J Med Sci Sports.* 2007;17(1):25–33.
12. Carvalho Alan PV, Vital Flávia MR, Soares B. Exercise interventions for shoulder dysfunction in patients treated for head and neck cancer. Chichester, UK: John Wiley & Sons, Ltd; 2010. Contract No: Report.
13. Cools AM, Dewitte V, Lanszweert F, Notebaert D, Roets A, Soetens B, et al. Rehabilitation of scapular muscle balance: which exercises to prescribe? ; 2007. Contract No: Report.
14. Mottram SL. Dynamic stability of the scapula. *Man Ther.* 1997;2(3):123.
15. Cools AM, Dewitte V, Lanszweert F, Notebaert D, Roets A, Soetens B, et al. Rehabilitation of scapular muscle balance which exercises to prescribe? *Am J Sports Med.* 2007;35(10):1744–51.
16. IJspeert J, Janssen RM, Murgia A, Pisters MF, Cup EH, Grootuis JT, et al. Efficacy of a combined physical and occupational therapy intervention in patients with subacute neuralgic amyotrophy: a pilot study. *NeuroRehabilitation.* 2013;33(4):657–65.
17. O'Brien M. Aids to the examination of the peripheral nervous system. Saunders-Elsevier; 2010. p. 66.
18. Mendell JR, Florence J. Manual muscle testing. *Muscle Nerve.* 1990;13(5):516–20.
19. Paternostro-Sluga T, Grim-Stieger M, Posch M, Schuhfried O, Vacariu G, Mittermaier C, et al. Reliability and validity of the Medical Research Council (MRC) scale and a modified scale for testing muscle strength in patients with radial palsy. *J Rehabil Med.* 2008;40(8):665–71.
20. Bohannon RW. Reference values for extremity muscle strength obtained by hand-held dynamometry from adults aged 20 to 79 years. *Arch Phys Med Rehabil.* 1997;78(1):26–32.
21. Kolber MJ, Beekhuizen K, Cheng MS, Fiebert IM. The reliability of hand-held dynamometry in measuring isometric strength of the shoulder internal and external rotator musculature using a stabilization device. *PhysiotherTheory Pract.* 2007;23(2):119.
22. Kolber MJ, Cleland JA. Strength testing using hand-held dynamometry. *Phys Ther Rev.* 2005;10(2):99.
23. Ekstrom RA, Bifulco KM, Lopau CJ, Andersen CF, Gough JR. Comparing the function of the upper and lower parts of the serratus anterior muscle using surface electromyography. *J Orthop Sports Phys Ther.* 2004;34(5):235–43.
24. Michener LA, Boardman ND, Pidcoe PE, Frith AM. Scapular muscle tests in subjects with shoulder pain and functional loss: reliability and construct validity. *Phys Ther.* 2005;85(11):1128–38.
25. Ekstrom RA, Donatelli RA, Soderberg GL. Surface electromyographic analysis of exercises for the trapezius and serratus anterior muscles. *The Journal of orthopaedic and sports physical therapy.* 2003;33(5):247–58.
26. Jung S-h, U-j H, Kim J-h, Gwak G-T, O-y K. Effects of horizontal shoulder abduction and adduction on the activity and strength of the scapular protractors. *J Electromyogr Kinesiol.* 2017;37:155–9.
27. Ekstrom RA, Soderberg GL, Donatelli RA. Normalization procedures using maximum voluntary isometric contractions for the serratus anterior and trapezius muscles during surface EMG analysis. *J Electromyogr Kinesiol.* 2005;15(4):418–28.
28. Park K-M, Cynn H-S, Yi C-H, Kwon O-Y. Effect of isometric horizontal abduction on pectoralis major and serratus anterior EMG activity during three exercises in subjects with scapular winging. *J Electromyogr Kinesiol.* 2013;23(2):462–8.
29. Van der Ploeg R, Oosterhuis H. The "make/break test" as a diagnostic tool in functional weakness. *J Neurol Neurosurg Psychiatry.* 1991;54(3):248–51.
30. Hermens HJ, Freriks B, Disselhorst-Klug C, Rau G. Development of recommendations for SEMG sensors and sensor placement procedures. *J Electromyogr Kinesiol.* 2000;10(5):361–74.
31. de Vet HC, Terwee CB, Knol DL, Bouter LM. When to use agreement versus reliability measures. *J Clin Epidemiol.* 2006;59(10):1033–9.
32. Koo TK, Li MY. A guideline of selecting and reporting Intraclass correlation coefficients for reliability research. *J Chiropr Med.* 2016;15(2):155–63.
33. de Vet HC, Terwee CB, Mokkink LB, Knol DL. Measurement in medicine: a practical guide: Cambridge University Press; 2011.
34. Bland JM, Altman DG. Measuring agreement in method comparison studies. *Stat Methods Med Res.* 1999;8(2):135–60.
35. Portney LG, Watkins MP. Foundations of clinical research: applications to practice. Upper Saddle River, NJ: Pearson/Prentice Hall; 2009.
36. Webb AL, O'Sullivan E, Stokes M, Mottram S. A novel cadaveric study of the morphometry of the serratus anterior muscle: one part, two parts, three parts, four? *Anat Sci Int.* 2016:1–10.
37. Kibler WB, McMullen J. Scapular dyskinesia and its relation to shoulder pain. *J Am Acad Orthop Surg.* 2003;11(2):142–51.
38. Stone CA, Nolan B, Lawlor PG, Kenny RA. Hand-held dynamometry: tester strength is paramount, even in frail populations. *J Rehabil Med.* 2011;43(9):808–11.
39. Kolber MJ, Beekhuizen K, M-SS C, Fiebert IM. The reliability of hand-held dynamometry in measuring isometric strength of the shoulder internal and external rotator musculature using a stabilization device. *Physiother Theory Pract.* 2007;23(2):119–24.
40. Winter D, Fuglevand A, Archer S. Crosstalk in surface electromyography: theoretical and practical estimates. *J Electromyogr Kinesiol.* 1994;4(1):15–26.
41. Fuglevand AJ, Winter DA, Patla AE, Stashuk D. Detection of motor unit action potentials with surface electrodes: influence of electrode size and spacing. *Biol Cybern.* 1992;67(2):143–53.
42. Mokkink LB, Terwee CB, Patrick DL, Alonso J, Stratford PW, Knol DL, et al. The COSMIN checklist for assessing the methodological quality of studies on measurement properties of health status measurement instruments: an international Delphi study. *Qual Life Res.* 2010;19(4):539–49.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.